Time scales of spike-train correlation for neural oscillators with common drive

Andrea K. Barreiro,* Eric Shea-Brown, and Evan L. Thilo

Department of Applied Mathematics, University of Washington, P.O. Box 352420, Seattle, Washington 98195, USA

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We examine the effect of the phase-resetting curve on the transfer of correlated input signals into correlated output spikes in a class of neural models receiving noisy superthreshold stimulation. We use linear-response theory to approximate the spike correlation coefficient in terms of moments of the associated exit time problem and contrast the results for type I vs type II models and across the different time scales over which spike correlations can be assessed. We find that, on long time scales, type I oscillators transfer correlations much more efficiently than type II oscillators. On short time scales this trend reverses, with the relative efficiency switching at a time scale that depends on the mean and standard deviation of input currents. This switch occurs over time scales that could be exploited by downstream circuits.

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I. INTRODUCTION

Throughout the nervous system, neurons produce spike trains that are correlated from cell-to-cell. This correlation or synchrony has received major interest because of its impact on how neural populations encode information. For example, correlations can strongly limit the fidelity of a neural code as measured by the signal-to-noise ratio of homogeneous populations [1–4]. However, the presence or stimulus dependence of correlations can also enhance coding strategies that rely on discriminating among competing populations [5–7]; in general, the effects of correlation on coding are complex and can be surprisingly strong [5–16]. In addition, stimulus-dependent correlations can modulate or carry information directly [17–24]. Correlations also play a major role in how signals are transmitted from layer-to-layer in the brain [25–27].

What is the origin of correlated spiking? One natural mechanism is the overlap in the inputs to different neurons these common inputs can drive common output spikes. This poses the question: how does the process of transferring of input correlations to spike train correlations depend on the nonlinear dynamics of individual neurons? Such *correlation transfer* has been modeled in integrate-and-fire-type neurons [20,27–31] and, very recently, in phase reductions in neural oscillators [32,33].

In particular, [32,33] contrast the correlated activity evoked in neural oscillators with type I (i.e., always positive) vs type II (i.e., positive and negative) phase-resetting curves (PRCs). When correlations are measured via equilibrium probability distributions of pairs of neuron phases or via cross-correlation functions of these phases over time, type II oscillators display relatively higher levels of correlation [32,33]. These results for phase correlation imply a similar finding for spike train correlation in the limit of very short time scales (the connection arises because the spike train cross-correlation function at $\tau=0$ can be related to the probability that phases will be nearly coincident for the two cells [34].) In this study, we also contrast correlation transfer in type I and type II oscillators (as well as in a continuum of intermediate models). The primary extension that we make is to study spike train correlation over a range of different time scales. Specifically, we measure the correlation coefficient ρ_T between the number of spikes produced by a pair of neurons in a time window of length *T*:

$$\rho_T = \frac{\operatorname{cov}(n_1, n_2)}{\sqrt{\operatorname{var}(n_1)}\sqrt{\operatorname{var}.(n_2)}}.$$
(1)

Here, n_1 and n_2 are the numbers of spikes output by neurons 1 and 2, respectively, in the time window; see Fig. 1 for an illustration.

We first derive a tractable expression for ρ_T in the long time scale limit $T \rightarrow \infty$ (cf. [20,30]). This can be given in terms of moments of an associated exit time problem. This reveals a dramatically higher level of long-time scale correlation transfer in type I vs type II neural oscillator models, the opposite of what was found in the earlier studies over short time scales (see Fig. 1). Next, we study ρ_T for successively shorter *T*, recovering the earlier findings of [32,33], and noting the critical time scale below which type II neurons become more efficient at transferring correlations. Additional results on how correlation transfer depends on neurons' operating range—that is, their spike rate and coefficient of variation (CV) of spiking—are developed as we go along.

II. MODELS OF NEURAL OSCILLATORS AND CORRELATION TRANSFER

A. Phase reductions

Neural oscillators can be classified into two types based on their intrinsic dynamics. Both types have the feature that as applied inputs (or "injected current") increases, the system transitions from a stable rest state to periodic firing through a bifurcation, the nature of which defines the type [35]. Here, as is often taken to be the case, type I neurons undergo a saddle node on invariant circle bifurcation, in which two fixed points collide and disappear, producing a periodic orbit that can have arbitrarily low frequency. Type II neurons undergo either a subcritical or supercritical Hopf bifurcation, in

^{*}akb6@washington.edu



FIG. 1. (Color online) (a) A schematic of the setup and correlation metric used in this study. Two cells receive both common and independent input, here modeled as white noise. Correlation of output spike trains is measured as the normalized covariance of spike counts over a finite time window *T* [see Eq. (5)]. (b) The principal result of our study; that correlation transfer efficiency depends on both internal dynamics and time scale of readout, with relative efficiency between type I (red or light gray) and type II (blue or dark gray) switching as readout time scale changes. The graph shows ρ_T for a particular set of model parameters (ω, σ) vs the measurement time window *T* (*T* is shown on a logarithmic scale). Insets show the phase-resetting curves used for the type I and type II models.

which a periodic orbit emerges at a nonzero minimum frequency.

Once the oscillator has passed through this bifurcation, it can be described by a single equation for its phase, in which inputs are mediated through a PRC which indicates the degree to which an input advances or delays the next spike. A PRC is derived for a mathematical model by phase reduction methods and determined experimentally by repeated perturbations of a system by input "kicks" [36]. Several investigators have demonstrated a connection between the type of bifurcation and the shape of the PRC: a type I oscillator PRC is everywhere positive so that positive injected current advances the time of the next spike [37], whereas a type II PRC has both positive and negative regions, so positive inputs advance or delay the next spike depending on their timing ([38]; see also [39]). Moreover, the form of type I and type II phase-resetting curves *near the bifurcation* are given by $(1 - \cos \theta)$ and $-\sin(\theta)$ respectively. We investigate these two PRCs, together with a family of PRCs given by a linear combination of these prototypical examples:

$$Z(\theta) = -\alpha \sin(\theta) + (1 - \alpha)[1 - \cos(\theta)], \quad 0 \le \alpha \le 1.$$
(2)

Here α homotopes the PRC from "purely" type I to type II; along the way, intermediate PRCs more representative of phase reductions of biophysical models are encountered [37,39,40]. For α =0, the phase model is exactly equivalent to the theta model and to the superthreshold quadratic integrate and fire model [38].

The question of how oscillators with different PRCs synchronize when they are coupled has been the subject of extensive study. Here, we ask about a different mechanism by which such oscillators can become correlated. Specifically, we consider an uncoupled pair of neurons receiving partially correlated noise. The dynamics have been reduced to a phase oscillator; each neuron is represented by a phase only. Each phase θ_i is governed by the stochastic differential equation

$$d\theta_i = \omega dt + \sigma Z(\theta_i) \circ (\sqrt{1 - c} dW_t^i + \sqrt{c} dW_t^c), \quad \theta_i \in (0, 2\pi),$$
(3)

where $\omega, \sigma > 0$, \circ denotes the Stratonovich integral, and

$$Z(\theta) = -\alpha \sin(\theta) + (1 - \alpha)[1 - \cos(\theta)]$$

Each θ_i receives independent white noise, dW_t^i , and common white noise dW_t^c is received by both. The noises are weighted so that the total variance of the noise terms in Eq. (3) is σ^2 . For the remainder of the paper, we treat the equivalent Itô integral

$$d\theta_{i} = \left(\omega + \frac{\sigma^{2}}{2}Z(\theta_{i})Z'(\theta_{i})\right)dt + \sigma Z(\theta_{i})dW_{i}, \quad \theta_{i} \in (0, 2\pi).$$
(4)

B. Measuring spike train correlation

We record spike times as those times t_i^k at which θ_i crosses 2π [37,38]. Because $Z(2\pi)=0$ and $\omega > 0$ for all the models we consider, θ always continues through 2π and begins the next period of interspike dynamics. We consider the output spike trains $y_i(t) = \sum_i \delta(t-t_i^k)$, where t_i^k is the time of the *k*th spike of the *i*th neuron. The firing rate of the *i*th cell, $\langle y_i(t) \rangle$, is denoted ν_i . As a quantitative measure of correlation over a given time scale *T*, we compute the following statistic:

$$\rho_T = \frac{\operatorname{cov}(n_1, n_2)}{\sqrt{\operatorname{var}(n_1)}\sqrt{\operatorname{var}(n_2)}},$$

where n_1 and n_2 are the numbers of spikes output by neurons 1 and 2, respectively, in a time window of length *T*; i.e., $n_i(t) = \int_t^{t+T} y_i(s) ds$.

By writing n_i in terms of a discretized spike train [i.e., $n_i = \sum_{t_1=t}^{t+T/\delta t} y_i(t_1)$] we can write ρ_T in terms of the autocorrelation and cross-correlation functions of y_i ; specifically

$$\rho_T = \frac{\int_{-T}^{T} C_{12}(t) \frac{(T-|t|)}{T} dt}{\sqrt{\int_{-T}^{T} C_{11}(t) \frac{(T-|t|)}{T} dt \int_{-T}^{T} C_{22}(t) \frac{(T-|t|)}{T} dt}},$$
 (5)

where $C_{ij}(\tau) = \langle y_i(t)y_j(t+\tau) \rangle - \nu_i \nu_j$ (see [41]; also Appendix A in [4]). It will be convenient for us to analyze the system in the Fourier domain. By the Wiener-Khinchin theorem, we can write Eq. (5) in terms of the power spectra $P_{ij} \equiv \langle \hat{y}_i^* \hat{y}_j \rangle$ as TIME SCALES OF SPIKE-TRAIN CORRELATION FOR ...

$$\rho_T = \frac{\int_{-\infty}^{\infty} P_{12}(f) K_T(f) df}{\sqrt{\int_{-\infty}^{\infty} P_{11}(f) K_T(f) df \int_{-\infty}^{\infty} P_{22}(f) K_T(f) df}},$$
(6)

where the kernel K_T is

$$K_T(f) = \frac{4}{Tf^2} \sin^2\left(\frac{Tf}{2}\right).$$

III. CORRELATION IN THE LONG TIME SCALE LIMIT

A. Linear-response theory for ρ_T

In this section we recall a derivation for a linear-response approximation to the spike train correlation; fuller discussion can be found in [20,30,42]. Assume that the fraction of noise variance c of the correlated input noise is small; then we treat the system with common noise as a perturbation to the system *without* common noise. Because the common noise is small, we will assume that the response of the system can be treated by linear-response theory; that is in the Fourier domain it can be characterized by a susceptibility function $A_{\omega,\sigma}(f)$ which gives the scaling factor between input and response at frequency f.

Specifically, we make the *ansatz* [42] that the Fourier transform can be written to lowest order in c

$$\hat{y}_i(f) = \hat{y}_{0,i}(f) + \sqrt{cA_{\omega,\sigma}(f)\hat{Q}(f)},$$

where $y_{0,i}$ is the spike output of the neuron without correlated noise, $\hat{Q}(f)$ is the Fourier transform of the correlated noise, and A is the susceptibility function. Then the crossspectrum of the two spike trains, $P_{12}(f)$, satisfies

$$P_{12}(f) = c |A_{\omega,\sigma}(f)|^2 \langle \hat{Q}^* \hat{Q} \rangle = c \sigma^2 |A_{\omega,\sigma}(f)|^2$$

as the base spike trains are independent of each other and the correlated noise Q, and taking the variance of Q to be σ^2 . Then at any finite T, ρ_T is linear in c, and (cf. [4,30]):

$$\rho_T(\omega,\sigma) = cS_T(\omega,\sigma) \tag{7}$$

$$=c\frac{\sigma^2 \int_{-\infty}^{\infty} |A_{\omega,\sigma}(f)|^2 K_T(f) df}{\sqrt{\int_{-\infty}^{\infty} P_{11}(f) K_T(f) df \int_{-\infty}^{\infty} P_{22}(f) K_T(f) df}}.$$
 (8)

Note that $S_T(\omega, \sigma)$ multiplies the input correlation *c* to yield the spike train correlation; for this reason we refer to $S_T(\omega, \sigma)$ as the correlation gain. We recover a simple expression for Eq. (6) in the limit $T \rightarrow \infty$. In the numerator, we converge to the value of the integrand at 0 as $f \rightarrow \infty$:

$$c\sigma^2 |A_{\omega,\sigma}(0)|^2$$
.

As $A_{\omega,\sigma}(0)$ is the limit of the susceptibility function as the frequency becomes arbitrarily small, it must be equivalent to the ratio of the dc response of the system (that is, the firing rate ν) to the strength of a constant dc input. Later we will use the symbol μ to include a dc input explicitly for the purposes of this computation. Therefore we define

$$\frac{d\nu}{d\mu} \equiv A_{\omega,\sigma}(0). \tag{9}$$

The denominator converges to $P_{11}(0)$ (assuming the unperturbed oscillators to be statistically identical) which for renewal processes is simply $\text{CV}^2\nu$.

Putting these results together, as $T \rightarrow \infty$, the finite-time correlations satisfy

$$\lim_{T \to \infty} \rho_T = c \frac{\sigma^2 \left(\frac{d\nu}{d\mu}\right)^2}{C V^2 \nu} \equiv c S(\omega, \sigma)$$
(10)

where ν is the mean output firing rate, CV is the coefficient of variation in the interspike intervals (ISIs), σ is the input noise amplitude. Each quantity can be computed from statistics of a single oscillator and combined to yield the long-time correlation gain $S(\omega, \sigma)$.

B. Computing moments of the exit time problem

The quantities ν , CV, and $\frac{d\nu}{d\mu}$ are related by moments of the ISIs and as such can be computed using the associated exit time problem. Specifically,

$$\nu = \frac{1}{T_1(0)},\tag{11}$$

$$CV = \frac{\sqrt{\{T_2(0) - [T_1(0)]^2\}}}{T_1(0)},$$
 (12)

$$\frac{d\nu}{d\mu} = -\frac{1}{(T_1(0))^2} \frac{dT_1(0)}{d\mu},$$
(13)

where $T_1(0)$ is the average time to cross $\theta = 2\pi$, given a start at $\theta_0 = 0$ (in other words, given a start at the last spike), and $T_2(0)$ is the second moment of this same quantity.

 $T_1(x)$ and $T_2(x)$ are given by solutions of the adjoint equation [43];

$$f_i(x) = A(x)\partial_x T_i + \frac{1}{2}B(x)\partial_x^2 T_i,$$
(14)

where

$$f_1(x) = -1, (15)$$

$$f_2(x) = -2T_1(x), \tag{16}$$

$$A(x) = \omega + \frac{\sigma^2}{2} Z(x) Z'(x), \qquad (17)$$

$$B(x) = \sigma^2 Z(x)^2, \tag{18}$$

and boundary conditions are given by $T_i(2\pi)=0$, $\partial T_i/\partial x$ bounded at x=0. The solution can be obtained by integrating Eq. (14) twice over the range $[0,2\pi]$, using the integrating factor Ψ :

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$$\Psi(x) = \exp\left[\int^{x} dx' \frac{2A(x')}{B(x')}\right], \quad \Psi(0) = 0.$$
(19)

If $\alpha = 0$, then B(x) has no interior zero and we proceed as follows:

$$\left[\Psi\frac{\partial T_i}{\partial x}\right]' = \frac{2f_i(x)}{B(x)}\Psi(x),\tag{20}$$

$$\frac{\partial T_i}{\partial x} = \frac{1}{\Psi(x)} \int_0^x \frac{2f_i(x')}{B(x')} \Psi(x') dx'.$$
(21)

If $\alpha > 0$ then B(x) has an interior zero at $\chi(\alpha)$, and we integrate separately on $(0, \chi(\alpha))$ and $(\chi(\alpha), 2\pi)$:

$$\frac{\partial T_i}{\partial x}(x) = \begin{cases} \frac{1}{\Psi(x)} \int_0^x \frac{2f_i(x')}{B(x')} \Psi(x') dx', & x < \chi(\alpha) \\ \frac{1}{\Psi(x)} \int_{\chi(\alpha)}^x \frac{2f_i(x')}{B(x')} \Psi(x') dx', & x > \chi(\alpha). \end{cases}$$
(22)

Finally $T_i(0)$ is given by a second integration

$$T_i(0) = \int_{2\pi}^0 \frac{\partial T_i}{\partial x}(x) dx.$$
 (23)

Here, the argument of the exponential function in $\Psi(x)$ can be any antiderivative of $\frac{2A(x)}{B(x)}$. $\Psi(0)$ [and $\Psi(\chi(\alpha))$, if $\alpha > 0$] is zero because the adjoint Eq. (14) has an irregular singularity at x=0 [and at $x=\chi(\alpha)$]; consequently $\frac{2A(x)}{B(x)} \to \infty$ and $\int^x dx \frac{2A(x)}{B(x)} \to -\infty$ as $x \to 0^+$ [and as $x \to \chi(\alpha)^+$]. This accounts for the difference between Eq. (23) and, for example, Eq. (5.2.157) in [43] [44]. Note that, also because Z(0)=0 and $\omega > 0$, x=0 is an entrance boundary so any exit must take place at 2π (i.e., an exit from the interval $(0, 2\pi)$ is equivalent to a spike).

For the class of PRCs that we consider, the antiderivative in Eq. (19) can be evaluated symbolically, therefore $\Psi(x)$ can be evaluated analytically. The integrals in Eqs. (21) and (23) must be evaluated by numerical quadrature.

We next discuss the integrability of Eqs. (21) and (22). First, we consider the case of the theta neuron (α =0), for which B(x) has only two zeros; at 0 and 2π . We can confirm the integrability by checking the following conditions:

$$\lim_{x \to 0^+} \int_0^x \frac{2f(x')}{B(x')} \Psi(x') dx' = 0,$$
(24)

$$\lim_{x \to 0^+} \Psi(x) = 0,$$
 (25)

$$\lim_{x \to 2\pi^{-}} \int_{0}^{x} \frac{2f(x')}{B(x')} \Psi(x') dx' = \pm \infty,$$
(26)

$$\lim_{x \to 2\pi^-} \Psi(x) = \infty.$$
 (27)

If these are satisfied then by l'Hôpital's rule,

$$\frac{\partial T_i}{\partial x} = \frac{1}{\Psi(x)} \int_0^x \frac{2f_i(x')}{B(x')} \Psi(x') dx'$$
(28)

is finite at the end points; in fact

$$\lim_{x \to 0} \frac{\partial T_i}{\partial x} = \lim_{x \to 0} \frac{f_i(x)}{A(x)},$$
(29)

$$\lim_{x \to 2\pi} \frac{\partial T_i}{\partial x} = \lim_{x \to 2\pi} \frac{f_i(x)}{A(x)},\tag{30}$$

and we can use a quadrature method that can handle integrable singularities. For $\alpha > 0$, B(x) has one interior zero, dividing the domain into two intervals on which Eq. (14) has irregular singularities at each end. Ψ must be computed separately on each interval. Again we find that $\frac{\partial T_i}{\partial x}$ is finite on each interval, permitting computation of Eq. (22) with a standard quadrature routine.

Finally, we compute the derivative of the firing rate with respect to a dc input; i.e., $\frac{\partial \nu}{\partial \mu}$ for the system

$$d\theta = \omega dt + Z(\theta)(\mu dt + \sigma \circ dW_t), \quad \theta \in [0, 2\pi), \quad (31)$$

which is equivalent to the Itô SDE

$$d\theta = \left(\omega + \frac{\sigma^2}{2}Z(\theta)Z'(\theta) + \mu Z(\theta)\right)dt + \sigma Z(\theta)dW_t,$$

$$\theta \in [0, 2\pi). \tag{32}$$

We wish to differentiate ν with respect to μ and evaluate at $\mu=0$. According to Eq. (13) we must evaluate $dT_1/d\mu(0,\mu)$ where the drift term $A(x,\mu) = \omega + \sigma^2/2Z(x)Z'(x) + \mu Z(x)$ is a function of both x and μ . In general, T_1 , T_2 , and Ψ are also functions of two arguments [e.g., $T_1(x,\mu)$], and we have indicated the arguments where needed for clarity. The notation $\frac{\partial}{\partial x}$ will refer to differentiation with respect to the first argument.

We first consider the case $\alpha=0$. Rewriting Eq. (23), we have

$$T_1(0,\mu) = \int_{2\pi}^0 \frac{1}{\Psi(x,\mu)} \int_0^x \frac{-2}{B(x')} \Psi(x',\mu) dx' dx, \quad (33)$$

where

$$\Psi(x,\mu) = \exp\left[\int^x \frac{2A(x',\mu)}{B(x')} dx'\right].$$
 (34)

Therefore,

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$$\frac{\partial T_1}{\partial \mu}(0,\mu) = \frac{d}{d\mu} \left(\int_{2\pi}^0 \int_0^x \frac{-2}{B(x')} \frac{\Psi(x',\mu)}{\Psi(x,\mu)} dx' dx \right) = \int_{2\pi}^0 \int_0^x \frac{-2}{B(x')} \frac{\Psi_\mu(x',\mu)\Psi(x,\mu) - \Psi_\mu(x,\mu)\Psi(x',\mu)}{\Psi(x,\mu)^2} dx' dx.$$
(35)

We use the relationship

$$\Psi_{\mu}(x,\mu) = \Psi(x,\mu) \int_{0}^{x} \frac{2}{B(y)} \frac{\partial A(y,\mu)}{\partial \mu} dy \qquad (36)$$

to find that

$$\frac{\partial T_1}{\partial \mu}(0,\mu) = \int_{2\pi}^0 \int_0^x \frac{2}{B(x')} \frac{\Psi(x',\mu)}{\Psi(x,\mu)} \int_{x'}^x \frac{2}{B(y)} \frac{\partial A(y,\mu)}{\partial \mu} dy dx' dx$$
$$= \int_{2\pi}^0 \int_0^x \int_0^y \frac{2}{B(x')} \frac{\Psi(x',\mu)}{\Psi(x,\mu)} \frac{2}{B(y)} \frac{\partial A(y,\mu)}{\partial \mu} dx' dy dx$$
(37)

assuming that the order of integration over x' and y can be switched. By Tonelli's theorem, this is valid if the integrand is single signed. For $\alpha = 0$, the integrand is always nonnegative [note that $\frac{\partial A}{\partial \mu}(x) = Z(x)$ and that B(x) is non-negative].

Next, we establish the integrability of expression (37). Rewriting, we have

$$\frac{\partial T_1}{\partial \mu}(0,\mu) = \int_{2\pi}^0 \frac{1}{\Psi(x,\mu)} \int_0^x \frac{2}{B(y)} \frac{\partial A}{\partial \mu} \Psi(y,\mu)$$
$$\times \frac{1}{\Psi(y,\mu)} \int_0^y \frac{2}{B(x')} \Psi(x',\mu) dx' dy dx$$
$$= \int_{2\pi}^0 \frac{1}{\Psi(x,\mu)} \int_0^x \frac{2}{B(y)} \frac{\partial A}{\partial \mu} \Psi(y,\mu) \frac{\partial T_1}{\partial x}(y) dy dx$$

As $\frac{\partial A}{\partial \mu}(x) = Z(x)$ and $\partial T_1 / \partial x$ are bounded, we can use the same conditions for integrability unchanged from Eqs. (24)–(27).

A parallel derivation to Eqs. (33)–(37) can be made when $\alpha > 0$. In this case we have

$$\frac{\partial T_1}{\partial \mu}(0,\mu) = \int_{2\pi}^0 \frac{\partial}{\partial \mu} \left(\frac{\partial T_1}{\partial x}(x,\mu)\right) dx,$$
(38)

where we have used the boundary condition $T_1(2\pi, \mu)=0$. The integrand is given by

$$\frac{\partial}{\partial\mu}\frac{\partial T_1}{\partial x}(x,\mu) = \begin{cases} \int_0^x \int_0^y \frac{2}{B(x')} \frac{\Psi(x',\mu)}{\Psi(x,\mu)} \frac{2}{B(y)} \frac{\partial A(y,\mu)}{\partial\mu} dx' dy, & x < \chi(\alpha) \\ \int_{\chi(\alpha)}^x \int_{\chi(\alpha)}^y \frac{2}{B(x')} \frac{\Psi(x',\mu)}{\Psi(x,\mu)} \frac{2}{B(y)} \frac{\partial A(y,\mu)}{\partial\mu} dx' dy, & x > \chi(\alpha). \end{cases}$$
(39)

Here, the switch in the order of integration is justified by the fact that the integrand $\frac{\partial A}{\partial \mu}$ is positive on $(0, \chi(\alpha))$ and negative on $(\chi(\alpha), 2\pi)$, while the range of integration in Eq. (39) is always restricted to lie in one region or the other.

C. Patterns of correlation transfer over long time scales

Having derived and shown how to evaluate formula (10), we next use it to evaluate spike count correlations ρ . The results are formally valid in the limits of time scale $T \rightarrow \infty$ and input correlation $c \rightarrow 0$ so we also conduct Monte Carlo simulations to reveal behavior of ρ_T for large but finite T and intermediate input correlation up to c=0.3 and to test the applicability of our formula in these regimes.

We compute these spike correlations over a range of ω and σ values that explores a full dynamical regime of the model. By this we mean that the values we use span from dominantly mean-driven firing (e.g., $\omega = 2.5$, $\sigma = 0.4$ at lower-right white square in Fig. 2), to dominantly fluctuation-

driven firing (e.g., $\omega = 0.4$, $\sigma = 2.4$ at upper-left white square) and all intermediate possibilities.

The resulting output firing rate ν for $\alpha=0$, computed via Eq. (11), ranges from 0 to 0.9 (measured in spikes per time unit); see Fig. 2 (left panel). Note that ν increases strongly with ω and only weakly with σ (see Sec. III D). The CV [via Eq. (12)] ranges from 0 to 0.55 (Fig. 2, right panel). As noted by [45,46], the superthreshold quadratic integrate and fire model—equivalent to our $\alpha=0$ phase model—has an upper bound on CV of $1/\sqrt{3} \approx .577$. By using a time change in the equations, CV can be seen to depend on the input parameters ω and σ only through the relationship $\tilde{\sigma}=\sigma/\sqrt{\omega}$ (see later in this section) and is therefore invariant on level curves of this ratio. As Fig. 2 shows, CV increases with this ratio.

We first fix a moderately long time window T=32, corresponding to 1.6–16 interspike intervals for the parameter range at hand, and compute ρ_T from Monte Carlo simulations for a range of correlation strengths $c \in [0, 0.3]$; see Fig. 3 (right column). We see that, for type I models, ρ_T is close to linear in this range of c, as for the linear-response theory. For



FIG. 2. Firing rate (left) and CV (right) of the theta model neuron (α =0) over a range of intrinsic phase speed ω and noise variance σ^2 . Sample spike trains are illustrated for four sets of (ω, σ) values (see white squares), notably mean-driven (high ω , low σ -bottom-most spike train) and fluctuation-driven (low ω , high σ -top-most spike train). Level sets of $\tilde{\sigma} = \frac{\sigma}{\sqrt{\omega}}$ are plotted (see text in Sec. III C).



FIG. 3. (Left) Susceptibility $S(\omega, \sigma)$ for global model parameter $\alpha = 0$ (top), $\alpha = 0.5$ (middle), and $\alpha = 1$ (bottom) over a range of intrinsic phase speed ω and noise variance σ^2 ; lines are level sets of $\tilde{\sigma} \equiv \sigma / \sqrt{\omega}$. (Right) Spike count correlation ρ_T vs fraction of correlated noise *c* from Monte Carlo simulations for $\alpha = 0$ (top), $\alpha = 0.5$ (middle), and $\alpha = 1$ (bottom). Error bars indicate the standard deviation over eight trials. The specific (ω, σ) values plotted are those shown in Fig. 2. ρ_T is measured over a time window of T=32 ms.



FIG. 4. Scatter plots of susceptibility $S(\omega, \sigma)$ vs firing rate ν (a) and susceptibility vs coefficient of variation (CV) (b) for global model parameter α =0 (light gray), α =0.5 (medium gray), and α =1 (black). $S(\omega, \sigma)$ was computed for the ranges of intrinsic phase speed ω and noise variance σ^2 shown in Fig. 3.

type II models, linearity holds over a decreased range of *c*. Additionally, note that the limiting formula Eq. (10) for ρ gives a close approximation to $\rho_{T=32}$ for type I models in more fluctuation-driven regimes. The approximation is worse for dominantly mean-driven firing, and for type II models, but the trend that correlations are lower for type II models is correctly predicted by Eq. (10).

Next, we discuss the trends in ρ predicted by the linearresponse theory. Two findings stand out in the left hand panels of Fig. 3. First, values of $S(\omega, \sigma)$ (and hence $\rho \approx Sc$) are much larger for type I (α =0) than for type II (α =1) models. Second, $S(\omega, \sigma)$ is nearly constant as the input mean and standard deviation ω and σ vary over a wide range, for both the type I and type II models. In sum, type I models transfer $\approx 66\%$ of their input correlations into spike correlations over long time scales; type II models transfer *none* of these input correlations, producing long-time scale spike counts that are uncorrelated. Additionally, an intermediate model (α =1/2) transfers an intermediate level of correlations, and these levels *do* depend on ω and σ . We will provide a partial explanation for overall trends in correlation transfer with α in Sec. III D.

Figure 4 provides an alternative view of these results by plotting the correlation gain S vs the firing rate and CV that are evoked by input parameters drawn from the whole range of ω, σ . First, note that S does not vary with firing rate for the type I or type II models, as expected from the previous plots. For the intermediate ($\alpha = 1/2$) model, S does not display a clear functional relationship with firing rate, but there is such a relationship with CV [Fig. 4(b)]. We note that all of these findings for the phase oscillators under study are in contrast to the behavior of linear integrate and fire neurons, which produce a strongly increasing, nearly functional relationship with firing rate [20,30]; we revisit this point in the discussion.

Now, we discuss a scaling relationship for the underlying equations that simplifies the parameter dependence and helps to explain the plots of *S* vs ν and *S* vs CV. This symmetry (which was noted in [45] for the quadratic integrate and fire model), allows us to reduce the free parameters ω, σ to one parameter $\tilde{\sigma} \equiv \sigma / \sqrt{\omega}$. The stochastic differential equation

$$d\theta_t = \left(\omega + \frac{\sigma^2}{2}Z(\theta)Z'(\theta) + \mu Z(\theta)\right)dt + \sigma Z(\theta)dW_t$$

becomes, under a time change $\tau = \omega t$,

$$d\theta_{\tau} = \left(1 + \frac{\sigma^2}{2\omega} Z(\theta) Z'(\theta) + \frac{\mu}{\omega} Z(\theta)\right) d\tau + \frac{\sigma}{\sqrt{\omega}} Z(\theta) dW_{\tau}$$
(40)

$$= \left(1 + \frac{\tilde{\sigma}^2}{2} Z(\theta) Z'(\theta) + \frac{\mu}{\omega} Z(\theta)\right) d\tau + \tilde{\sigma} Z(\theta) dW_{\tau}.$$
 (41)

Each exit time must scale identically under this transformation so that the exit time moments scale as

$$\widetilde{T}_1 = \omega T_1 \to \widetilde{\nu} = \frac{\nu}{\omega},\tag{42}$$

$$\tilde{T}_2 = \omega^2 T_2, \tag{43}$$

and therefore the $CV = \sqrt{\tilde{T}_2 - \tilde{T}_1^2/\tilde{T}_1}$ is invariant under the time change. Thus, the CV, which is computed with $\mu = 0$, depends only on $\tilde{\sigma}$, not on ω and σ separately. Now consider the two sets of parameters (ω, σ) and $(1, \tilde{\sigma})$, such that $\tilde{\sigma} = \sigma/\sqrt{\omega}$. According to Eq. (41), the effect of μ is scaled by $1/\omega$ so that

$$\frac{d\tilde{\nu}}{d\mu} = \frac{1}{\omega} \frac{d\nu}{d\mu}.$$
(44)

Therefore, the susceptibility

$$S(\omega,\sigma) = \frac{\sigma^2 \left(\frac{d\nu}{d\mu}\right)^2}{CV^2\nu}$$
(45)

$$=\frac{\sigma^2 \frac{1}{\omega^2} \left(\frac{d\tilde{\nu}}{d\mu}\right)^2}{\widetilde{\mathrm{CV}}^2 \frac{\tilde{\nu}}{\omega}}$$
(46)

$$= \frac{\sigma^2}{\omega} \frac{\left(\frac{d\tilde{\nu}}{d\mu}\right)^2}{\widetilde{CV}^2\tilde{\nu}}$$
(47)

$$=S(1,\tilde{\sigma}) \tag{48}$$

is invariant under the change in parameters $(\omega, \sigma) \rightarrow (1, \sigma/\sqrt{\omega})$; exactly the same change in parameters under which the CV is conserved. Therefore, if there is a single contour for each value of CV (i.e., there are no disconnected contours), we expect that *S* will be a function of CV, as in Fig. 4(b). Conversely, note that the firing rate will vary widely over any particular $\tilde{\sigma}$ contour so that many different firing rates can be expected to yield the same *S*; unless *S* is constant, we expect a given firing rate to be associated with a range of *S* values, as also seen in Fig. 4(a). The uniqueness of CV level sets for $\alpha=0$ is previously known [46].

Finally, in Fig. 5, we demonstrate that the behavior of *S* seems to roughly "interpolate" between the $\alpha = 0, 1/2, 1$ cases considered here as it varies over the whole range of α . *S* typically decreases as the total noise variance σ increases.

D. Analytical arguments for type I vs type II difference in correlation gain S

We now seek to explain the drop in $S(\omega, \sigma)$ [Eq. (10)] as α increases, ranging from type I (α =0) to type II (α =1) PRCs. There are two tractable limits in which explicit calculations can be performed. First, we show that $S(\omega, \sigma)$ =0 for "purely" type II models, for any values of ω and σ . Next, for arbitrary α , we derive an $S(\omega, \sigma)$ valid to first order in σ^2 —this reveals a monotonic decrease in *S* with α and gives a good description of correlation transfer even for $\sigma \approx 1$. Fi-

nally, we give an intuitive argument to buttress these calculations.

1. S=0 for purely type II models

We start with $\alpha = 1$. It is straightforward to see that $d\nu/d\mu = 0$ for any ω, σ . Recall that $d\nu/d\mu$ is given by the integral of a function over the interval $(0, 2\pi)$, in Eq. (38); we will show this function integrates to zero. Rewriting Eq. (39), using $\chi(1) = \pi$,

$$\frac{\partial}{\partial \mu} \frac{\partial T_1}{\partial x} = \begin{cases} \frac{1}{\Psi(x,\mu)} \int_0^x \frac{2}{B(y)} \frac{\partial A}{\partial \mu}(y,\mu) \Psi(y,\mu) \times \frac{\partial T_1}{\partial x}(y,\mu) dy, & x < \pi \\ \frac{1}{\Psi(x,\mu)} \int_{\pi}^x \frac{2}{B(y)} \frac{\partial A}{\partial \mu}(y,\mu) \Psi(y,\mu) \times \frac{\partial T_1}{\partial x}(y,\mu) dy, & x > \pi. \end{cases}$$
(49)

 $\Psi(x,\mu)$, B(x), and $\frac{\partial T_1}{\partial x}(x,\mu)$ are each π periodic [i.e., $f(x) = f(x+\pi)$]. $\frac{\partial A}{\partial \mu} \equiv Z(x) = -\sin(x)$, however, is antiperiodic $[f(x) = -f(x+\pi)]$. Then

$$\frac{\partial}{\partial\mu}\frac{\partial T_1}{\partial x}(x,\mu) = -\frac{\partial}{\partial\mu}\frac{\partial T_1}{\partial x}(x+\pi,\mu)$$
(50)

and integrating $\frac{\partial}{\partial \mu} \left[\frac{\partial T_1}{\partial x}(x,\mu) \right]$ over a full period $x \in (0, 2\pi)$ yields zero. Plugging this into Eq. (10), we see that $S(\omega,\sigma) \equiv 0$ for models with type II PRCs $Z(\theta) = -\sin(\theta)$ (ν and CV are always nonzero in this paper).

2. Evaluation of $S(\omega, \sigma)$ in the limit $\sigma \rightarrow 0$

We next derive an analytical expression for $S(\omega, \sigma)$ in the limit $\sigma \rightarrow 0$. We will show that each relevant term $T_1(0)$, $T_2(0)$, and $\frac{\partial T_1}{\partial \mu}(0)$ admits an asymptotic expansion in the small parameter σ^2 . We compute these terms explicitly and combine them to get the first term of the associated expansion for $S(\omega, \sigma)$.



FIG. 5. Susceptibility $S(1, \sigma)$ for a continuum of models specified by $\alpha \in [0, 1]$.

If we examine the integral in Eq. (21) and the inner integral of Eq. (35) for $\alpha=0$ or the integrals in Eq. (22) and Eq. (39) for $\alpha>0$, we see that we can write each of them in the form

$$\frac{1}{Z(y)} \int_{a}^{y} f(x') \exp\left\{\frac{1}{\sigma^{2}} [F(x') - F(y)]\right\} dx', \qquad (51)$$

where F(x') is strictly increasing on (a, y). *a* may be either 0 or χ_{α} , depending on the circumstance. This integral admits an asymptotic expansion in σ^2 , with successive terms essentially given by integrating by parts and retaining only the contribution from the end of the interval where F(x')-F(y) = 0. In the case of $T_1(x)$ we have

$$f(y) = \frac{1}{Z(y)}$$

In the case of $T_2(x)$ we have

$$f(y) = \frac{T_1(y)}{Z(y)}$$

and for $d\nu/d\mu$

$$f(y) = \frac{\partial T_1}{\partial x}(y)$$

In each case F(x') is given by the antiderivative of $2\omega/Z(x')^2$; because this is a positive function on $(0, \chi(\alpha))$ and $(\chi(\alpha), 2\pi)$, F(x') must clearly be increasing on these intervals. The integral

$$\int_{a}^{b} f(x') \exp(\lambda \phi(x')) dx'$$
 (52)

admits the following expansion for $\lambda \rightarrow \infty$, if $\phi' > 0$ on [a,b] and f meets certain conditions (see, for example, [47],):



FIG. 6. $\lim_{\sigma\to 0^+} S(1,\sigma)$ for a continuum of models specified by $\alpha \in [0,1]$ (dashed black line). This is a good approximation for small (σ =0.2; dark gray line) and moderate (σ =1; light gray line) values of σ .

$$I(\lambda) \sim \sum_{n=0}^{\infty} \frac{(-1)^n}{\lambda^{n+1}} \Biggl\{ \exp[\lambda \phi(x)] \Biggl[\frac{1}{\phi'(x)} \frac{d}{dx} \Biggr]^n \frac{f(x)}{\phi'(x)} \Biggr\}_a^b.$$
(53)

If $\phi(x) \rightarrow -\infty$ as $x \rightarrow a$, as is the case in our use of the formula, only the right-hand end point makes a contribution to the integral.

Substituting this contribution into the outer integral and evaluating these quantities to the required order, we find

$$T_1(0) = \frac{2\pi}{\omega} + O(\sigma^4),$$
 (54)

$$T_2(0) = \frac{4\pi^2}{\omega^2} + \sigma^2 \left(\frac{\pi}{\omega^3} (3 - 6\alpha + 4\alpha^2)\right) + O(\sigma^4), \quad (55)$$

$$\frac{dT_1}{d\mu}(0) = -\frac{2\pi}{\omega}(1-\alpha) + O(\sigma^4).$$
 (56)

In passing, we note that the firing rate gain, $d\nu/d\mu$, is given by

$$\frac{d\nu}{d\mu} = -\frac{1}{T_1(0)^2} \frac{dT_1}{d\mu}(0)$$
(57)

$$=\frac{1-\alpha}{2\pi}+O(\sigma^4). \tag{58}$$

Putting these results together we see that

$$S(\omega, \sigma) = \frac{2(1-\alpha)^2}{3-6\alpha+4\alpha^2} + O(\sigma^2).$$
 (59)

It can be readily checked that this function decreases monotonically from a value of 2/3 at $\alpha = 0$, to a value of 0 at $\alpha = 1$.

While this calculation is in the limit $\sigma \rightarrow 0^+$, it in fact remains a good approximation for moderate σ , in fact, even for $\sigma \sim \omega$. Figure 6 shows the limiting value as well as computed *S* values at small (relative to $\omega = 1$; $\sigma = 0.2$) and moderate ($\sigma = 1$) values of σ . The limiting value remains a good approximation throughout this range.

3. Argument for general PRCs

We close this by section by noting that, for arbitrary PRCs $Z(\theta)$ and small σ ,

$$d\nu/d\mu \propto \int_0^{2\pi} Z(\theta) d\theta.$$

The calculations showing this are in the appendix. While $S(\omega, \sigma) = \sigma^2 (d\nu/d\mu)^2/CV^2\nu$ has other terms that depend on the PRC, this calculation does suggest that *S* is likely to be smaller for PRCs with lower means in general, and lends some intuition to what drives the decrease in *S* with α .

IV. CORRELATION OVER SHORTER TIME SCALES

Figure 7 shows ρ_T computed for a sequence of finite time windows *T*. We can characterize the nondimensional *T* in terms of its length in terms of a typical interspike interval (ISI) of the oscillator. The time window *T*=1 varies from 0.05–0.5 ISI, roughly, from left to right; the time window *T*=32 varies from 1.6–16 ISI.

We see a striking dependence of transferred correlations on T. ρ_{32} is larger for type I than for type II oscillators for most parameter values, consistent with our long time results.

However, $\rho_1(\omega, \sigma)$ is smaller for type I than for type II for 95% of parameter pairs (ω, σ) . This is consistent with recent results on the response of phase oscillators to correlated noise [32,33]; in particular [32], study the distribution of phase difference $\Delta \theta \equiv \theta_1 - \theta_2$ between two oscillators driven by common noise and find that the probability that $\Delta \theta = 0$ is greater for type II than for type I. As noted in the Introduction, this metric can be shown to have a direct relationship with our ρ_T as $T \rightarrow 0$. To summarize, the "switch" in $S_T(\omega, \sigma)$ (from higher correlation gain in type II models to higher correlation gain in type II models are biologically relevant, as we discuss in the next section.

V. SUMMARY AND DISCUSSION

We asked how correlated input currents are transferred into correlated spike trains in a class of nonlinear phase models that are generic reductions in neural oscillators. Linearresponse methods, asymptotics, and Monte Carlo simulations gave the following answers:

(1) Over long time scales, type I oscillators transfer 66% of incoming current correlations into correlated spike counts, while type II oscillators transfer almost *none* of their input correlations into spike count correlations. Models with intermediate phase response curves transfer intermediate levels of correlations.

(2) Over long time scales, correlation transfer in type I and type II models is independent of the rate and coefficient of variation (CV) of spiking. For intermediate models, correlation transfer decreases with CV and shows no clear dependence on rate.

(3) That there is a time scale *T* beneath which these results *reverse*: type II neurons become more efficient at trans-



FIG. 7. Spike count correlation $\rho_T(\omega, \sigma)$ as measured from Monte Carlo simulations with global model parameter $\alpha = 0$ (top row), $\alpha = 0.5$ (middle row), and $\alpha = 1$ (bottom row). Measurement time intervals are, from the leftmost column, T=1, T=2, T=8, and T=32 (ms). ρ_T is computed for a range of intrinsic phase speed ω and noise variance σ^2 . The fraction of noise variance that is received by both oscillators is c=0.1; therefore, to recover the approximate susceptibility $S_T(\omega, \sigma) \approx \rho_T(\omega, \sigma)/c$, multiply by 10. As *T* increases, S_T approaches the $T \rightarrow \infty$ limit illustrated in Fig. 3.

ferring correlations than type I, there is an increasing dependence of correlation transfer on spike rate, and the strong dependence on CV weakens.

We note that results (1) and (2) are highly distinct from findings for the leaky integrate-and-fire neuron model, for which up to 90%-100% of correlations are transferred over long time scales, with this level depending strongly on firing rate but very weakly on CV [20,30]. This demonstrates a strong role for subthreshold dynamics in determining correlation transfer in the oscillatory regime (as seen for the quadratic integrate-and-fire model in [30]).

What time scales of spike count correlation actually matter in a given application? This depends on the circuit that is "downstream" of the pair (or, similarly, layer) of neural oscillators that we have studied in this paper; in other words, on what system is *reading out* the neurons we study here. Clearly, different neurons and networks are sensitive to input fluctuations over widely varying time scales. For example, some single neurons and circuits can respond only to events in which many of the cells that provide inputs spike nearly simultaneously. This is the coincidence detector mode of operation (cf. [48] and references therein) and can result from fast membrane time constants (as occur in high-conductance states [49]); circuit mechanisms, such as feed-forward inhibition [50], can also play a role. For such systems, short-time scale correlations among upstream cells are relevant-small window lengths T. On the opposite extreme, networks operating as neural integrators will accumulate inputs over arbitrarily long time scales (see [51] and references therein); in this case, spike-time correlations over large windows T are reflected in circuit activity. In general there is a range of possible behaviors, and the time scales over which inputs are integrated can differ among various components of a network, among components of an individual cell [48,50] or among different times in a cell lifetime, depending on background input characteristics [49].

One domain in which different levels of correlation transfer-and different dependences of this correlation transfer on neurons' operating ranges-can have a strong effect is the population coding of sensory stimuli. For example, if neurons are read out over long time scales, then type I vs type II populations offer a choice between relatively high and low levels of correlation across the population. Depending on heterogeneity of the population response to the stimulus at hand, one or the other of these choices can yield dramatically greater (Fisher) information about the encoded stimulus [1,5,15]. The opposite choice of neuron type would be preferred for readout over short time scales, where trends in correlation transfer reverse. Beyond averaged levels of correlation, a separate question that can affect encoding is whether correlations depend on the stimulus [24,52]. A natural way that this can occur is when correlations depend on the evoked rate or CV of firing. We demonstrate that such dependencies are present in phase models over short time scales and, over long time scales, that they are present in intermediate but not "purely" type-I or type-II models. Once again, depending on details of stimulus encoding, these dependencies can either enhance or degrade encoding. Overall, the picture that emerges is that correlation transfer is another factor to consider in asking which nonlinearities allow neuron models to best encode stimuli, and that there will be different answers for different stimuli.

In closing, we note that we have studied only simple (but widely-used) one-dimensional neural models here. However, preliminary simulations suggest that the trends for correlation transfer found here also hold in some standard type-I vs type-II conductance-based neuron models [35]. The situation is more complex, as global features of the neural dynamics can be involved, and will be explored in future work.

APPENDIX

In this appendix we give some more details about calculation of $T_1(0)$, $T_2(0)$, and $dT_1/d\mu(0)$ for specific values of α .

1. $\alpha = 1$ and numerical details

For
$$Z(x) = -\sin(x)$$
 ($\alpha = 1$),

$$A(x) = \omega + \frac{\sigma^2}{2}\sin(x)\cos(x), \qquad (A1)$$

$$B(x) = \sigma^2 [\sin(x)]^2 \tag{A2}$$

are periodic on $[0, \pi]$ with B(x)=0 at $O(2\pi)$ and π .

 $\Psi(x)$ is defined as an antiderivative as in Eq. (19); we can compute this symbolically yielding

$$\Psi(x) = \sin(x)\exp\left(-\frac{2\omega}{\sigma^2}\cot(x)\right).$$
 (A3)

We can check that $\lim_{x\to 0^+} \Psi(x)=0$, $\lim_{x\to \pi^-} \Psi(x)=\infty$, and that Ψ/B is not integrable at either 0 or π .

For the interval π to 2π we use the fact that A(x) and B(x) are π periodic; Ψ repeats on this second interval; that is,

$$\Psi(x) = |\sin(x)| \exp\left(-\frac{2\omega}{\sigma^2} \cot(x)\right)$$
(A4)

is an expression that is valid everywhere $Z(\theta) \neq 0$.

To compute values of $\partial T_1 / \partial x$ on a uniform mesh, we use an adaptive quadrature routine to evaluate Eqs. (22); in particular Simpson's rule implemented via the MATLAB routine quad. We have already demonstrated the integrability of Eqs. (22) in Sec. III B. $T_1(0)$ is then computed using Simpson's three-point rule.

To compute values of $\partial T_2 / \partial x$, we use adaptive quadrature as well, with the caveat that $\partial T_1 / \partial x$ is evaluated in between mesh points by linear interpolation.

2. $\alpha = 0$

For the theta model, $Z(x) = 1 - \cos(x)$ or $\alpha = 0$,

$$A(x) = \omega + \frac{\sigma^2}{2} [1 - \cos(x)] \sin(x), \qquad (A5)$$

$$B(x) = \sigma^2 [1 - \cos(x)]^2$$
 (A6)

are periodic on $[0, 2\pi]$ with B(x)=0 at $O(2\pi)$. Again we can integrate 2A(x)/B(x) symbolically, finding

$$\Psi = |1 - \cos(x)| \exp\left\{-\frac{2\omega}{3\sigma^2} \frac{[2 - \cos(x)]\sin(x)}{[1 - \cos(x)]^2}\right\}.$$
 (A7)

We can verify Eq. (24) as before.

3. Small σ argument for general PRC

Here we replicate the small σ value of $d\nu/d\mu$, using a perturbation expansion valid for an arbitrary PRC.

We consider the stationary densities $p(\theta)$ and $\hat{p}(\theta)$ of two different processes,

$$d\theta = a(\theta)dt + b(\theta)dW_t, \tag{A8}$$

$$d\hat{\theta} = \hat{a}(\theta)dt + b(\theta)dW_t, \tag{A9}$$

where

$$a(\theta) = \omega + \frac{\sigma^2}{2} Z(\theta) Z'(\theta), \qquad (A10)$$

$$\hat{a}(\theta) = \omega + \frac{\sigma^2}{2} Z(\theta) Z'(\theta) + \mu Z(\theta), \qquad (A11)$$

 $p(\theta)$ satisfies the stationary Fokker-Planck equation

$$-\frac{\partial}{\partial\theta}(ap) + \frac{\partial^2}{\partial\theta^2}(bp) = 0$$
 (A12)

This can be integrated and the constant of integration is equal to the firing rate:

$$ap - \frac{\partial}{\partial \theta}(bp) = \nu$$
 (A13)

and therefore

$$\nu = \frac{1}{2\pi} \int_0^{2\pi} a(\theta) p(\theta) d\theta, \qquad (A14)$$

$$\hat{\nu} = \frac{1}{2\pi} \int_0^{2\pi} \hat{a}(\theta) \hat{p}(\theta) d\theta.$$
(A15)

The dc input response, $d\nu/d\mu$, can be computed by differentiating $\hat{\nu}$ with respect to μ and evaluating at $\mu=0$. Therefore we expand $\hat{\nu}$ as a series in μ and take the first-order term

$$\hat{p} = p + \mu p_1 + O(\mu^2),$$
 (A16)

$$\hat{\nu} = \nu + \mu \nu_1 + O(\mu^2).$$
 (A17)

We find that

$$\frac{d\nu}{d\mu} = \nu_1 = \frac{1}{2\pi} \left[\int_0^{2\pi} p(\theta) Z(\theta) d\theta + \int_0^{2\pi} p_1(\theta) a(\theta) d\theta \right].$$
(A18)

We consider Eq. (A18) more carefully. We will see that all but one term are multiplied by σ^2 ; for small σ , the term that remains significant is the mean of the phase-resetting curve. We rewrite Eq. (A18) as follows:

$$\nu_{1} = \frac{1}{2\pi} \left[\int_{0}^{2\pi} \left(\frac{1}{2\pi} + \tilde{p}(\theta) \right) Z(\theta) d\theta + \sigma^{2} \int_{0}^{2\pi} \frac{1}{2} Z(\theta) Z'(\theta) p_{1}(\theta) d\theta \right]$$
(A19)

$$= \frac{1}{2\pi} \left[\int_{0}^{2\pi} \frac{1}{2\pi} Z(\theta) d\theta + \int_{0}^{2\pi} \tilde{p}(\theta) Z(\theta) d\theta + \sigma^{2} \int_{0}^{2\pi} \frac{1}{2} Z(\theta) Z'(\theta) p_{1}(\theta) d\theta \right]$$
(A20)

using the fact that $p_1(\theta)$ must average to 0 so that \hat{p} remains a probability density. We have also written $p(\theta)$, the stationary density for the process with $\mu=0$, as the sum of a uniform density and a deviation $\tilde{p}(\theta)$.

Consider the process

$$d\theta = \left(\omega + \frac{\sigma^2}{2}Z(\theta)Z'(\theta)\right)dt + \sigma Z(\theta)dW_t.$$
 (A21)

The stationary density *p* and firing rate *J* satisfy

$$\left(\omega + \frac{\sigma^2}{2} Z(\theta) Z'(\theta)\right) p(\theta) - \frac{\partial}{\partial \theta} \left(\frac{\sigma^2}{2} Z^2(\theta) p(\theta)\right) = J.$$
(A22)

If $\sigma=0$ then the stationary density is $p_0=\frac{1}{2\pi}$ and $J_0=\frac{\omega}{2\pi}$. We expand p and J in powers of σ^2 ;

$$p(\theta) = p_0 + \tilde{p} \tag{A23}$$

$$=p_0 + \sigma^2 \tilde{p}_1 + O(\sigma^4), \qquad (A24)$$

$$J = J_0 + \sigma^2 J_1 + O(\sigma^4).$$
 (A25)

At O(1) we have

$$p_0 = \frac{J_0}{\omega} \tag{A26}$$

as already stated. At $O(\sigma^2)$

$$\widetilde{p}_1 = \frac{1}{\omega} \left(J_1 + \frac{Z^2}{2} \frac{\partial p_0}{\partial \theta} + \frac{1}{2} Z Z' p_0 \right)$$
(A27)

$$=\frac{1}{\omega}\left(J_1 + \frac{1}{4\pi}ZZ'd\theta\right),\tag{A28}$$

 J_1 is determined so that p is a probability density at any order:

$$\int_{0}^{2\pi} J_1 = 2\pi J_1 = -\frac{1}{4\pi} \int_{0}^{2\pi} ZZ' d\theta = 0 \qquad (A29)$$

as ZZ' is the perfect derivative of a periodic function. For general order, we have

$$\widetilde{p}_n = \frac{1}{\omega} \left[J_n - \frac{1}{2} Z Z' \widetilde{p}_{n-1} + \frac{\partial}{\partial \theta} \left(\frac{Z^2}{2} \widetilde{p}_{n-1} \right) \right], \quad (A30)$$

$$J_n = \frac{1}{4\pi} \int_0^{2\pi} Z Z' \tilde{p}_{n-1} d\theta, \qquad (A31)$$

where we no longer expect J_n to be zero.

Let's return to Eq. (A20). The first integral is the mean of $Z(\theta)$. The second integral, in our expansion, first appears at fourth-order in σ . To see this, we examine

$$\int_{0}^{2\pi} \widetilde{p}_{1} Z(\theta) d\theta = \frac{1}{4\pi} \int_{0}^{2\pi} Z^{2}(\theta) Z'(\theta) d\theta \qquad (A32)$$

(A33)

The third term is second-order in σ . Thus the dominant term in Eq. (A20) is the first one, and we have shown the desired result.

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- [1] E. Zohary, M. Shadlen, and W. Newsome, Nature (London) **370**, 140 (1994).
- [2] K. O. Johnson, J. Neurophysiol. 43, 1793 (1980).
- [3] K. H. Britten, M. N. Shadlen, W. T. Newsome, and J. A. Movshon, J. Neurosci. 12, 4745 (1992).
- [4] W. Bair, E. Zohary, and W. T. Newsome, J. Neurosci. 21, 1676 (2001).
- [5] L. F. Abbott and P. Dayan, Neural Comput. 11, 91 (1999).
- [6] B. B. Averbeck, P. E. Latham, and A. Pouget, Nat. Rev. Neurosci. 7, 358 (2006).
- [7] R. Romo, A. Hernandez, A. Zainos, and E. Salinas, Neuron 38, 649 (2003).
- [8] Y. Chen, W. S. Geisler, and E. Seidemann, Nat. Neurosci. 9, 1412 (2006).
- [9] J. Poort and P. R. Roelfsema, Cereb. Cortex (to be published).
- [10] M. W. Oram, P. Földiák, D. I. Perrett, and F. Sengpiel, Trends Neurosci. 21, 259 (1998).

- [11] P. Seriès, P. E. Latham, and A. Pouget, Nat. Neurosci. 7, 1129 (2004).
- [12] A. Kohn, M. A. Smith, and J. A. Movshon, *Computational and Systems Neuroscience* (Cold Spring Harbor, New York, 2004).
- [13] M. Shamir and H. Sompolinsky, Neural Comput. 16, 1105 (2004).
- [14] M. Shamir and H. Sompolinsky, Neural Comput. 18, 1951 (2006).
- [15] H. Sompolinsky, H. Yoon, K. Kang, and M. Shamir, Phys. Rev. E 64, 051904 (2001).
- [16] E. Schneidman, M. J. Berry, R. S. II, and W. Bialek, Nature (London) 440, 1007 (2006).
- [17] R. C. deCharms and M. M. Merzenich, Nature (London) 381, 610 (1996).
- [18] J. M. Samonds, J. D. Allison, H. A. Brown, and A. B. Bonds, J. Neurosci. 23, 2416 (2003).
- [19] A. Kohn and M. A. Smith, J. Neurosci. 25, 3661 (2005).

- [20] J. de la Rocha, B. Doiron, E. Shea-Brown, K. Josic, and A. Reyes, Nature (London) 448, 802 (2007).
- [21] C. M. Gray, P. K. A. K. Engel, and W. Singer, Nature (London) 338, 334 (1989).
- [22] J. Biederlack, M. Castelo-Branco, S. Neuenschwander, D. W. Wheeler, W. Singer, and D. Nikolić, Neuron 52, 1073 (2006).
- [23] M. J. Chacron and J. Bastian, J. Neurophysiol. **99**, 1825 (2008).
- [24] K. Josic, E. Shea-Brown, B. Doiron, and J. de la Rocha, Neural Comput. 21, 2774 (2009).
- [25] E. Salinas and T. Sejnowski, J. Neurosci. 20, 6193 (2000).
- [26] A. Kuhn, A. Aertsen, and S. Rotter, Neural Comput. 15, 67 (2003).
- [27] T. Tetzlaff, S. Rotter, E. Stark, M. Abeles, A. Aertsen, and M. Diesmann, Neural Comput. 20, 2133 (2008).
- [28] M. D. Binder and R. K. Powers, J. Neurophysiol. 86, 2266 (2001).
- [29] R. Moreno-Bote and N. Parga, Phys. Rev. Lett. 96, 028101 (2006).
- [30] E. Shea-Brown, K. Josić, J. de la Rocha, and B. Doiron, Phys. Rev. Lett. **100**, 108102 (2008).
- [31] M. Shadlen and W. Newsome, J. Neurosci. 18, 3870 (1998).
- [32] S. Marella and G. Ermentrout, Phys. Rev. E 77, 041918 (2008).
- [33] R. F. Galan, G. B. Ermentrout, and N. N. Urban, Phys. Rev. E 76, 056110 (2007).
- [34] B. Pfeuty, G. Mato, D. Golomb, and D. Hansel, Neural Comput. 17, 633 (2005).
- [35] J. Rinzel and G. Ermentrout, in *Methods in Neuronal Modeling*, edited by C. Koch and I. Segev (MIT Press, Cambridge, MA, 1998), pp. 251–291.

- [36] A. Winfree, *The Geometry of Biological Time* (Springer, New York, 2001).
- [37] G. Ermentrout, Neural Comput. 8, 979 (1996).
- [38] G. Ermentrout and N. Kopell, SIAM J. Math. Anal. 15, 215 (1984).
- [39] E. Brown, J. Moehlis, and P. Holmes, Neural Comput. **16**, 673 (2004).
- [40] D. Hansel, G. Mato, and C. Meunier, Europhys. Lett. 23, 367 (1993).
- [41] D. Cox and P. Lewis, *The Statistical Analysis of a Series of Events* (John Wiley, London, 1966).
- [42] B. Lindner, B. Doiron, and A. Longtin, Phys. Rev. E 72, 061919 (2005).
- [43] C. Gardiner, Handbook of Stochastic Methods, Series in Synergetics, 3rd ed. (Springer, New York, 2004).
- [44] The expression we obtain is identical to the evaluation of this expression in the case of a reflecting boundary at 0.
- [45] B. Lindner, A. Longtin, and A. Bulsara, Neural Comput. 15, 1761 (2003).
- [46] R. Vilela and B. Lindner, J. Theor. Biol. 257, 90 (2009).
- [47] N. Bleistein and R. Handelsman, Asymptotic Expansions of Integrals (Dover, New York, 1986).
- [48] M. Rudolph and A. Destexhe, J. Comput. Neurosci. 14, 239 (2003).
- [49] A. Destexhe, M. Rudolph, and D. Paré, Nat. Rev. Neurosci. 4, 739 (2003).
- [50] F. Pouille and M. Scanziani, Science 293, 1159 (2001).
- [51] C. Brody, R. Romo, and A. Kepecs, Curr. Opin. Neurobiol. 13, 204 (2003).
- [52] S. Panzeri, S. R. Schultz, A. Treves, and E. T. Rolls, Proc. R. Soc. London, Ser. B 266, 1001 (1999).